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LABORATORY STUDY

FAILURE

RENAL

The effects of transdermal insulin treatment of streptozotocin-induced diabetic rats on kidney function and renal expression of glucose transporters

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Abstract

The tight glycemic control required to attenuate chronic complications in type 1 diabetes mellitus requires multiple daily injections of bolus insulin which cause hyperinsulinemic edema and hypertension due to Na⁺ retention. Reports indicate that pectin insulin (PI)-containing dermal patches sustain controlled insulin release into the bloodstream of streptozotocin (STZ)induced diabetic rats. This study investigated whether PI dermal patches can improve the impaired renal function in diabetes. PI patches were prepared by dissolving pectin/insulin in deionized water and solidified with CaCl₂. Short-term (five weeks) effects of thrice daily treatments with PI patches on renal function and urinary glucose outputs were assessed in diabetic animals. Blood and kidney samples were collected after five weeks for measurements of selected biochemical parameters. Blood was also collected for insulin measurement 6 h following treatments. The low plasma insulin concentrations exhibited by STZ-induced diabetic rats were elevated by the application of insulin-containing dermal patches to levels comparable with control non-diabetic rats. Untreated STZ-induced diabetic rats exhibited elevated urinary glucose, K⁺ outputs and depressed urinary Na⁺ outputs throughout the 5-week period. Treatment with PI dermal patches increased urinary Na⁺ output and reduced urine flow, urinary glucose and K⁺ excretion rates in weeks 4 and 5. PI dermal patches increased GFR of diabetic rats with concomitant reduction of plasma creatinine concentrations. Transdermal insulin treatment also decreased the renal expressions of GLUT1 and SGLT1 of STZ-induced diabetic rats. We conclude that PI dermal patches deliver physiologically relevant amounts of insulin that can improve kidney function in diabetes.

Keywords

Diabetes, GLUT1, hyperglycemia, insulin, kidney function, pectin, SGLT1, transdermal

History

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Introduction

Hyperglycemia leads to the development and progression of end-stage renal disease (ESRD), the principal cause of death as a result of diabetic nephropathy (DN). Clinical trials suggest that there is no effective treatment for diabetic nephropathy and the prevention of the occurrence and progression of DN have become a serious medical challenge.¹ DN is precipitated directly or indirectly via four main molecular mechanisms which include oxidative stress, protein kinase C (PKC), polyol/aldose reductase and advanced glycation end product (AGE)-receptor of AGE (RAGE) pathways and the renin-angiotensin system.² These pathways metabolize excess glucose to toxic metabolites that perturb intra-renal hemodynamics via glycosylation of intra-renal proteins which induce hyperfiltration and glomerular dysfunction.³⁻⁵ Much emphasis on diabetes care and management is on optimal blood glucose control to avert these adverse outcomes. Literature evidence indicates that intensive insulin therapy either via multiple daily injections or continuous subcutaneous insulin (sc insulin) infusion is more effective in protecting renal function than conventional insulin therapy.^{6,7} The main limitations of these treatments include adherence to diet, particularly as regards to carbohydrate ingestion, the most important measure in avoiding hypoglycemic events. Furthermore, reports indicate that the intensive therapy is associated with increased Na⁺ retention resulting in hyperinsulinemic edema and hypertension.⁸ Other therapeutic interventions such as metformin, insulin secretagogues do not achieve glycemic targets and thus the search for new treatment strategies is ongoing. We have reported that insulin-containing dermal patch formulation sustains slow controlled release of insulin into the bloodstream of diabetic rats with a concomitant reduction of blood glucose concentrations.9 The focus of this paper was to determine whether sustained controlled insulin release from insulin-containing dermal patches can improve the impaired renal fluid and electrolyte handling of streptozotocin (STZ)-induced diabetic rats. Several studies have reported compromised renal function in experimental diabetes^{10,11} and diabetic patients.^{12–14}

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The insulin-responsive facilitative glucose transporters, SGLT1 and GLUT1 found in the proximal convoluted tubule are responsible for re-absorbing filtered glucose from the tubule back into circulation.¹⁵ These co-transporters are up-regulated in the diabetic kidney^{16,17} and result in greater re-absorption of glucose and thus contributing to the preexisting hyperglycemia. The up-regulation of these transporters has been implicated in the pathogenesis of progressive diabetic nephropathy.¹⁸ Accordingly, we determined whether transdermally delivered insulin has any effect on renal expression of glucose transporters of STZ-induced diabetic rats. The study was designed to establish whether application of pectin insulin-containing dermal patches which sustain controlled release of insulin into the bloodstream of STZ-induced diabetic rats can modulate kidney dysfunction associated with diabetes mellitus as assessed by effects on renal fluid and electrolyte handling in STZ-induced diabetic rats.

Materials and methods

Drugs and chemicals

Amidate low-methoxyl pectin with a degree of methoxylation (DM) of 23, degree of amidation (DE) of 24 was donated by Dr Hans-Ulrich Endress of Herbstreith and Fox KG, Neuenburg, Germany. Drugs were sourced from standard pharmaceutical suppliers. All other chemicals which were of analytical grade quality were purchased from standard commercial suppliers.

Pectin insulin (PI) patch preparation

The amidated pectin hydrogel matrix patch was prepared using a previously described protocol described by Musabayane et al. with slight modifications.¹⁹ Briefly, amidated low methoxyl pectin was dissolved in deionized water (4 g/100 mL) and mixed with agitation for 30 min. Subsequently, DMSO (3 mL), eucalyptus oil (1.5 mL), vitamin E (1.5 mL) and puromycin (100 μ L) were added to the mixture which was left to mix with agitation for another 30 min after which various amounts of insulin (Novo Rapid Pen Refill, Novo Nordisk Pty Ltd., Sandton, South Africa) were added and mixed with agitation in separate beakers in water bath at 37 °C for 15 min. Following this, an aliquot of the mixture (11 mL) was transferred to a petri dish with a known diameter and a 2% CaCl₂ solution was added on top of pectin and left to stand at room temperature for 10 min to allow for cross-linking and hence formation of the matrix patch. Preliminary studies indicated that the patches contained 1.20, 2.87 and 5.04 µg of insulin which translated to dosages of 3.99, 9.57 and 16.80 µg/kg, respectively.

Dissolution studies

The pectin hydrogel matrix dermal patches of the same size were dissolved in Sorenson's phosphate buffer (pH 7.2) to determine the amount of insulin incorporated. The percentage uptake of insulin into the patch was calculated by dividing the theoretical insulin uptake by the actual insulin measured.

Animals

Male Sprague-Dawley rats (250–300 g, bred at the Biomedical Research Unit, University of KwaZulu-Natal)

were used in this study. The animals were kept and maintained under standard laboratory conditions of temperature, humidity, 12 h day:12 h night cycle and allowed water *ad libitum* and given 30 g standard rat chow daily (Meadow Feeds, Pietermaritzburg, South Africa). All animal experimentation was reviewed and approved by the Animal Ethics Committee of the University of KwaZulu-Natal (102/11/ Animal).

Induction of diabetes mellitus

Type 1 diabetes mellitus was induced by a single intraperitoneal injection of 60 mg/kg STZ in freshly prepared 0.1 M citrate buffer (pH 6.3). Control group received the vehicle, citrate buffer through the same route. Animals that exhibited glucosuria after 24 h, tested by urine strips (Rapidmed Diagnostics, Sandton, South Africa) were considered diabetic. Seven days later, the blood glucose concentration of STZinduced diabetic rats greater than 20 mmol/L was considered as indicating stable diabetes.

Application of the hydrogel patch

Rats were shaved on the dorsal region of neck 1–2 days prior to the application of PI hydrogel matrix patches. The dermal patches were secured in place with adhesive hydro film (Hartman-Congo Inc., Rock Hill, South Carolina, USA) and rat jackets (Braintree, Scientific, Inc., Braintree, Massachusetts, USA) which were adjusted for the size of the animal.

Short-term studies

Studies were conducted in groups of STZ-induced diabetic rats housed individually in Makrolon polycarbonate metabolic cages (Tecniplast, Labotec, South Africa) over a 5-week period. Various doses of insulin (3.99, 9.57 and 16.80 μ g/kg) were applied topically thrice daily via PI insulin matrices onto the shaved skin area on the back of the neck skin at 09 h00 followed by the same dose at 17 h00 and the 8 h later (01 h00). Animals treated with drug-free pectin and sc insulin (175 μ g/kg) acted as negative and positive controls, respectively. The amounts of food and water consumed were recorded daily at 09 h00. The weights of the animals were measured once every week.

Renal studies

Urine volume and urinary concentrations of glucose, creatinine, urea, Na⁺, K⁺ and Cl⁻ were determined daily while mean arterial blood pressure (MAP) was monitored every third consecutive day using non-invasive tail cuff method with photoelectric sensors (IITC Model 31 Computerized Blood Pressure Monitor, Life Sciences, Woodland Hills, CA). The unit works with IITC hardware system to measure blood pressure and heart rate in conscious rats. The animals were warmed at ± 30 °C in an enclosed chamber (IITC Model 303sc Animal Test Chamber IITC Life Sciences, Woodland Hills, CA) for 30 min before taking blood pressure readings. All measurements were conducted at 09h00. Blood samples were collected by cardiac puncture into individual pre-cooled heparinized containers at the end of the 5-week experimental period for biochemical analysis. Glomerular filtration rate (GFR), as assessed by creatinine clearance ($C_{\rm Cr}$) was calculated using the standard formulae from measurements of the plasma and urinary concentrations of creatinine and urine flow rate in the fifth week.

Urinalysis

Urine flow was determined gravimetrically. Na⁺, K⁺, urea and creatinine were analyzed using the Beckman Coulter Counter (Synchron CX3 Clinical Systems, Fullerton, California, USA) with commercial diagnostic kits from Beckman Coulter, Dublin Ireland. Glucose was measured using a glucometer (Bayer's Glucometer Elite[®] Elite (Pty) Ltd., Health Care Division, Isando, South Africa).

Laboratory analyses insulin

At the end of 6 h following treatment with various doses of PI patches (3.99, 9.57 and 16.80 μ g/kg); animals were sacrificed by exposing to halothane for 3 min via a gas anaesthetic chamber (100 mg/kg). Blood was collected by cardiac puncture into pre-cooled heparinized tubes for insulin determination. The plasma insulin concentrations were measured by ultrasensitive rat insulin ELISA kit (DRG Instruments GmBH, Marburg, Germany). The immunoassay is a quantitative method utilizing two monoclonal antibodies which together are specific for insulin. The lower limit of detection was 1.74 pmol/L. The intra- and inter-assay analytical coefficients of variation ranged from 4.4 to 5.5% and from 4.7 to 8.9%, respectively.

Arginine vasopressin

Blood samples for arginine vasopressin (AVP) measurements were also collected and treated as described for insulin from STZ-induced diabetic rats after five weeks of transdermal treatment with PI patch. Plasma AVP concentrations were determined by standard enzymatic methods using an arg⁸vasopressin ELISA Kit (Abcam, Cambridge, Massachusetts, USA). The lower and upper limits of detection were 4 pmol/L and 923 pmol/L, respectively. The intra-assay analytical coefficient of variation ranged from 5.9 to 10.6% and the inter-assay coefficient variation from 6.0 to 8.5%. In all cases, rats treated with insulin free pectin patch or sc insulin $(175 \,\mu g/kg)$ acted as untreated and treated positive controls, respectively (n=6 in each group). Separated plasma was analyzed for AVP, Na⁺, K⁺, creatinine and urea concentrations. Glomerular filtration rate (GFR), as assessed by creatinine clearance (C_{Cr}) was calculated using the standard formulae from measurements of the plasma and urinary concentrations of creatinine and urine flow rate in the fifth week.

Kidney histology

At the end of the five weeks, control non-diabetic, untreated STZ-induced diabetic rats and treated STZ-induced diabetic rats were killed by exposing to halothane via a gas anaesthetic chamber. Kidneys were excised and fixed in 10% formaldehyde solution, rehydrated in decreasing grades of ethanol and embedded in paraffin wax. These samples $(3-5 \,\mu\text{m} \,\text{thick})$

were sectioned with a micro rotary microtome (Robert-Bosch-Stra β e, Walldorf, Baden-Württemberg, Germany). The sections were then cleared in xylene and rehydrated in decreasing concentrations of ethanol. Subsequently, the sections were stained with hematoxylin and eosin (H and E), washed and dehydrated in increasing grades of ethanol and cleared in xylene. The processed sections were viewed and captured using a Leica Scanner, SCN400 and Slide Path Gateway LAN software for analysis (Leica Microsystems CMS, Wetzlar, Germany).

SGLT1 and GLUT1

Kidney tissues (0.1 g) were homogenized on ice in isolation buffer (0.5 mm Na₂EDTA, 0.1 M KH₂PO₄, 0.1 mmol dithiothreitol, 0.25 M sucrose) and then centrifuged at $400 \times g$ for 10 min (4 °C) for SGLT1 and GLUT1 analyses. The protein content for all samples was standardized to one concentration (1 mg/mL) was quantified using the Lowry method.²⁰ The proteins were then denatured by boiling in Laemmli sample buffer (0.5 M Tris-HCl, glycerol, 10% sodium dodecyl sulfate (SDS), 2-mercaptoethanol, 1% bromophenol blue) for 5 min. The denatured proteins were loaded $(25 \,\mu\text{L})$ on prepared resolving (10%) and stacking (4%) polyacrylamide gels along with molecular weight marker (5 μ L). The gel was electrophoresed for 1 h at 150 V in electrode (running) buffer (Trisbase, glycine, SDS, pH 8.3). Following electrophoresis, the resolved proteins were electro-transferred to an equilibrated polyvinylidene difluoride (PVDF) membrane for 1 h in transfer buffer (192 mm glycine, 25 mm tris, 10% methanol). After transfer, the membrane was blocked with 5% non-fat dry milk in Trisbuffered saline with 0.1% Tween 20 (TTBS) (20 mm tris, 150 mm NaCl, KCl, 0.05% Tween-20). The membrane was then immune-probed with antibodies-SGLT1 and GLUT1 (catalogue numbers ab99447, ab15309, respectively, Abcam, Cambridge, United Kingdom, 1:1000 in 1% BSA, Neogen, USA) for 1 h at room temperature. The PVDF membrane was then subjected to five washes (10 min each with gentle agitation) with TTBS. Following which, the membrane was incubated in horse radish peroxidase (HRP)-conjugated secondary antibody (rabbit anti-mouse 1:10,000; Bio-Rad) for 1 h at RT. After further washing, antigen-antibody complexes were detected by chemiluminescence using the Immune-star[™] HRP substrate kit (Bio-Rad, Johannesburg, South Africa). Chemiluminescent signals were detected with the Chemi-doc XRS gel documentation system and analyzed using the quantity one software (Bio-Rad, Johannesburg, South Africa). Band intensity analysis was conducted on the resultant bands.

Statistical analysis

Data are presented as the means \pm standard error of mean (SEM). Overall statistical comparisons between the control means and experimental groups were performed with GraphPad InStat Software (version 5.00, GraphPad Software, San Diego, California, USA), using one-way analysis of variance (ANOVA), followed by Tukey-Kramer multiple comparison test. A value of p < 0.05 was considered significant. The test which assumes equal variance for the

three or more means is generally used to determine whether the means differ significantly in an analysis of variance.

Results

Insulin-loading efficiency

The loading efficiency of insulin in amidated pectin insulincontaining dermal patches ranged from 76% to 94% and patches used contained 1.20, 2.87 and 5.04 μ g of insulin, respectively, which translated to a dosage of 3.99, 9.57 and 16.80 μ g/kg, respectively.

Short-term effects of PI

Body weight, food and water intake

Table 1 compares daily weight changes, 24 h food and water intake by control non-diabetic and STZ-diabetic rats and PI-treated STZ-diabetic rats over the 5-week experimental period. Untreated diabetic rats exhibited characteristic signs of diabetes such as severe wasting and increased intake of water. There was no difference in food intake as animals were given a standard amount of food (30 g/day). Treatment with PI hydrogel matrix patches with low doses of insulin (3.99 and 9.57 μ g/kg) significantly reduced the weight loss and water intake from week 4 while the highest dose (16.80 μ g/kg) and sc insulin (175 μ g/kg, sc) effects were observed from week 1.

Renal fluid and electrolyte handling

Untreated STZ-induced diabetic rats exhibited high volumes of weekly urine output and increased urinary K^+ output throughout the 5-week study compared with non-diabetic control animals (Table 2). On the other hand, urinary Na⁺ output of diabetic rats was significantly reduced (Table 2). Application of insulin-containing dermal patches with high insulin doses (16.80 µg/kg) significantly increased urinary Na⁺ outputs of diabetic rats from week 4. On the other hand PI insulin treatment reduced the volume of urine voided and urinary K⁺ output of STZ-diabetic rats, but higher than in control non-diabetic animals by the end of the 5th week. The PI-induced loss of Na⁺ was not reflected in the plasma by the end of the experimental period although plasma K⁺ concentration was reduced by comparison with untreated diabetic rats (Table 3). Urinary creatinine and urea outputs of diabetic rats were significantly (p < 0.05) reduced by comparison with non-diabetic control rats (data not shown). However, plasma creatinine concentrations were significantly (p < 0.05) elevated in control STZ-induced diabetic rats by comparison with untreated non-diabetic rats at the end of the 5-week experimental period (Table 3). The PI hydrogel matrix patch with highest insulin (16.80 μ g/kg) significantly (p < 0.05) reduced plasma creatinine concentration in STZ-induced diabetic rats concomitant increase in GFR (Table 3). The plasma urea concentration after five weeks with the highest dose patch was 82% of that in untreated STZ-induced diabetic rats (p < 0.05). The transdermal PI hydrogel matrix patches $(3.99, 9.57 \text{ and } 16.80 \,\mu\text{g/kg})$ decreased the MAP by the end of the 5-week experimental period (Table 3).

Terminal hormone measurements

Plasma insulin and AVP concentrations of untreated STZinduced diabetic rats were significantly low (p < 0.05) at end of the 5-week experimental period by comparison with control non-diabetic animals (Table 3). Treatment with insulin-containing dermal patches at various doses over a 5-week period significantly (p < 0.05) elevated plasma insulin concentrations of STZ-induced rats in a dose-independent manner. The application of insulin-containing dermal patch (16.80 µg/kg) as well as insulin (175 µg/kg, sc) restored the

Table 1. Comparisons of the effects of insulin-containing dermal patches on body weight, food and water intake in STZ-induced diabetic rats with control non-diabetic animals and untreated diabetic rats.

		Week					
	Group	1	2	3	4	5	
Measure	Non-diabetic control	11 ± 2	11 ± 1	12 ± 1	11 ± 1	12 ± 1	
Food intake (g/100 g)	STZ-diabetic untreated	12 ± 1	13 ± 2	13 ± 1	13 ± 2	14 ± 1	
<i>.e e,</i>	STZ-diabetic (3.99)	11 ± 1	12 ± 1	11 ± 1	12 ± 2	12 ± 1	
	STZ-diabetic (9.57)	13 ± 2	12 ± 1	11 ± 1	12 ± 1	11 ± 1	
	STZ-diabetic (16.80)	11 ± 1	11 ± 1	11 ± 1	12 ± 2	11 ± 1	
	STZ-diabetic (sc insulin)	12 ± 1	11 ± 1	11 ± 1	11 ± 2	11 <u>±</u> 1	
Water intake (mL/100 g)	Non-diabetic control	11 ± 1	13 ± 1	12 ± 2	12 ± 1	13 ± 2	
	STZ-diabetic untreated	$59 \pm 1*$	$52 \pm 2^{*}$	$55 \pm 2^{*}$	$59 \pm 1^{*}$	$64 \pm 2^{*}$	
	STZ-diabetic (3.99)	$58 \pm 1*$	$59 \pm 1^{*}$	$53 \pm 1^{*}$	$52 \pm 1^{*}$	$58 \pm 1^{*}$	
	STZ-diabetic (9.57)	$59 \pm 2^{*}$	$56 \pm 1^{*}$	$54 \pm 2^{*}$	$59 \pm 1^{*}$	$57 \pm 1^{*}$	
	STZ-diabetic (16.80)	$55 \pm 1^{*}$	$53 \pm 2^{*}$	$55 \pm 1^{*}$	$53 \pm 1^{*}$	$52 \pm 1^{*}$	
	STZ-diabetic (sc insulin)	$54 \pm 1^*$	$59 \pm 3^*$	$53 \pm 1^{*}$	—	$59 \pm 1*$	
% b.wt change	Non-diabetic control	7 ± 1	6 ± 1	8 ± 1	13 ± 2	22 ± 1	
C	STZ-diabetic untreated	$-9 \pm 1^{*}$	$-7 \pm 2^{*}$	$-9 \pm 1^{*}$	$-8 \pm 2^{*}$	$-9 \pm 1^{*}$	
	STZ-diabetic (3.99)	$-6 \pm 1^{*}$	$-3 \pm 1^{\circ}$	$2 \pm 1^{*}$	4±1*◊	3±1*◊	
	STZ-diabetic (9.57)	$-7 \pm 1^{*}$	$-2\pm1*\diamond$	4±1*◊	$3 \pm 1^{*}$	2±1*◊	
	STZ-diabetic (16.80)	3±1*◊	4±1*◊	4±1*◊	$3 \pm 1^{*}$	$4 \pm 2^{*}$	
	STZ-diabetic (sc insulin)	$6\pm1\diamond$	$3 \pm 1^{*\diamond}$	$4 \pm 2^{*}$	$2\pm1^{*}\diamond$	$3\pm1*\diamond$	

Notes: Insulin was administered thrice daily for five weeks via dermal PI patches or subcutaneous injection. Data are expressed as mean \pm SEM, n = 6 in each group.

*Denotes p < 0.05 by comparison with control non-diabetic animals at the corresponding period.

 \diamond Denotes p < 0.05 by comparison with control STZ-induced diabetic rats at the corresponding period.

Table 2. Comparison of the effects of insulin-containing dermal patches on renal function parameters in STZ-induced diabetic rats with control non-diabetic animals and untreated diabetic rats.

		Time (weeks)					
Parameter	Group	1	2	3	4	5	
Urine volume (mL/day)	Non-diabetic control	12 ± 1	14 ± 1	14 ± 1	14 ± 1	14 ± 1	
	STZ-diabetic untreated	$94 \pm 3^{*}$	$97 \pm 3^{*}$	$116 \pm 3^*$	$119 \pm 2^*$	$121 \pm 2*$	
	STZ-diabetic (3.99)	$93 \pm 2^{*}$	$93 \pm 3^{*}$	$112 \pm 3^*$	$117 \pm 4*$	$119 \pm 3^{*}$	
	STZ-diabetic (9.57)	$90 \pm 3^{*}$	$98 \pm 2^*$	$114 \pm 3^{*}$	$114 \pm 2^{*}$	$118 \pm 2^{*}$	
	STZ-diabetic (16.80)	$94 \pm 3^{*}$	$101 \pm 2^*$	$115 \pm 1*$	$108 \pm 2^{*} \bullet \diamond$	106±1*•◊	
	STZ-diabetic(sc insulin)	$94 \pm 2^*$	$101 \pm 2^*$	$115 \pm 3*$	$108 \pm 2^{*} \bullet \diamond$	$106 \pm 2^{*} \bullet \diamond$	
Urinary K ⁺ excretion	Non-diabetic control	4.41 ± 0.23	5.41 ± 0.30	4.23 ± 0.22	4.20 ± 0.20	3.30 ± 0.30	
(mmol/day)	STZ-diabetic untreated	$8.41 \pm 0.21*$	$9.30 \pm 0.21^{*}$	$8.44 \pm 0.34*$	$9.70 \pm 0.11^*$	$8.44 \pm 0.12^{*}$	
	STZ-diabetic (3.99)	$8.31 \pm 0.24*$	$7.10 \pm 0.91^{*}$	5.34 ± 0.31*◊	6.23 ± 0.24*◊	6.20±0.31*◊	
	STZ-diabetic (9.57)	$7.40 \pm 0.91^{*}$	$6.99 \pm 0.95^{*}$	6.01 ± 0.33*◊	6.11 ± 0.34*◊	6.10±0.23*◊	
	STZ-diabetic (16.80)	$5.33 \pm 0.32^{\circ}$	$6.40 \pm 0.83^{\circ}$	$5.30 \pm 0.34^{\circ}$	$4.53 \pm 0.24 * \bullet \diamond$	$4.13 \pm 0.32^{*} \bullet \diamond$	
	STZ-diabetic (sc insulin)	5.43 ± 0.20*◊	5.30±0.2*◊	5.20±0.34*◊	$4.80 \pm 0.22^{*} \bullet \diamond$	4.14±0.22*•◊	
Urinary Na ⁺ excretion	Non-diabetic control	12.32 ± 0.31	13.30 ± 0.24	14.17 ± 0.32	13.50 ± 0.24	14.24 ± 0.36	
(mmol/day)	STZ-diabetic untreated	$4.43 \pm 0.30^{*}$	$4.33 \pm 0.24*$	$5.50 \pm 0.35*$	$5.54 \pm 0.25^{*}$	$6.40 \pm 0.20^{*}$	
	STZ-diabetic (3.99)	$4.22 \pm 0.30^{*}$	$5.42 \pm 0.32^{*}$	$5.12 \pm 0.24*$	$5.80 \pm 0.20^{*}$	$6.17 \pm 0.23^{*}$	
	STZ-diabetic (9.57)	$4.90 \pm 0.21^{*}$	$5.10 \pm 0.23^{*}$	$5.41 \pm 0.20^{*}$	$5.58 \pm 0.25^{*}$	$6.33 \pm 0.31^{*}$	
	STZ-diabetic (16.80)	$4.40 \pm 0.30^{*}$	$5.24 \pm 0.20^{*}$	$6.77 \pm 0.24^{*}$	$7.84 \pm 0.32^{*} \bullet \diamond$	$8.90 \pm 0.20^{*} \bullet \diamond$	
	STZ-diabetic (sc insulin)	$4.40 \pm 0.21^{*}$	$5.11 \pm 0.31^*$	$6.24 \pm 0.30^{*}$	$7.40 \pm 0.25^{*} \bullet \diamond$	8.24±0.20*•◊	

Notes: Insulin was administered thrice daily for five weeks via dermal PI patches or subcutaneous injection. Data are expressed as mean \pm SEM, n = 6 in each group.

*Denotes p < 0.05 by comparison with respective non-diabetic control animals.

 \diamond Denotes p < 0.05 by comparison with respective STZ-diabetic control animals.

•Denotes p < 0.05 by comparison with (3.99 and 9.57 µg/kg) doses.

Table 3. Comparisons of the effects on terminal plasma biochemical parameters of insulin-containing dermal patches in STZ-induced diabetic rats with control non-diabetic and untreated diabetic rats.

	Group						
Parameter	Non-diabetic control	STZ-diabetic untreated	STZ-diabetic (3.99)	STZ-diabetic (9.57)	STZ-diabetic (16.80)	STZ-diabetic (sc insulin)	
Na ⁺ (mmol/L)	141 ± 2	138 ± 3	144 ± 2	143 ± 3	144 ± 4	144 ± 3	
K ⁺ (mmol)	3.90 ± 0.20	$7.30 \pm 0.30*$	$6.90 \pm 0.20*$	$6.21 \pm 0.32^*$	5.40±0.41◊	$7.10 \pm 0.42*$	
Urea (mmol/L)	7.31 ± 0.92	9.82 ± 1.43	8.62 ± 0.98	9.11 ± 0.94	8.04 ± 0.72	8.41 ± 0.81	
Creatinine (µmol/L)	25.23 ± 1.12	$37.50 \pm 1.24*$	$36.14 \pm 0.94*$	$35.82 \pm 1.14*$	33.31 ± 0.75*◊	31.21 ± 0.93*◊	
GFR mL/min/100 g	0.85 ± 0.11	$0.41 \pm 0.12*$	0.69 ± 0.12	$0.71 \pm 0.22 \diamond$	0.81 ± 0.31 \$	0.74 ± 0.20 \$	
MAP (mmHg)	105 ± 2	$119 \pm 2^{*}$	$104 \pm 1\diamond$	97 ± 1◊	99 ± 2◊	104 ± 1	
Kidney weight (g/100 g)	0.46 ± 0.02	0.35 ± 0.01	0.33 ± 0.02	0.32 ± 0.01	0.36 ± 0.01	0.37 ± 0.01	
Glucose (mmol/L)	5.30 ± 0.30	$29.40 \pm 2.10^{*}$	13.30 ± 2.30*↔	9.50 ± 2.10*◊	6.60 ± 0.11	$5.90 \pm 0.10 $	
Insulin (ng/mL)	8.40 ± 0.34	$2.50 \pm 0.38^{*}$	$5.50 \pm 0.28 $	6.21 ± 0.15*◊	6.53 ± 0.17*◊	$7.28 \pm 0.25^{*}$	
AVP (pmol/L)	431 ± 3	152±4 *	Not measured	Not measured	$326 \pm 5 \diamond$	521 ± 3◊	

Notes: Insulin was administered thrice daily for five weeks via subcutaneous injection or PI insulin matrices. Data are expressed as mean \pm SEM, n = 6 in each group.

*Denotes p < 0.05 by comparison with respective non-diabetic control animals.

 \diamond Denotes p < 0.05 by comparison with respective STZ-diabetic control animals.

concentration of AVP to levels comparable to values of nondiabetic control animals (Table 3).

Effects of PI hydrogel patch on urinary glucose

Transdermal application of PI matrix patch at a dose of $16.80 \,\mu$ g/kg for five weeks significantly (p < 0.05) decreased blood glucose and urinary glucose output of STZ-induced diabetic rats (Figure 1, Table 3). To evaluate whether reduction in urinary glucose output was mediated via modulation of insulin-responsive facilitative glucose transporters, the effects of transdermal insulin on glucose transporters expression, renal GLUT1 and SGLT1 were analyzed for using western blotting in kidney tissues harvested from

STZ-induced diabetic rats at the end of 5-week study. The expression of GLUT1 and SGLT1 was significantly increased in STZ-induced diabetic animals in comparison to non-diabetic controls (Figure 2). Similar to sc insulin, the insulincontaining dermal patch normalized GLUT1 and SGLT1 expression. Kidney mass was not altered by transdermal insulin treatment (Table 3).

PI effects on kidney histology

Untreated non-diabetic rat kidney sections (Figure 3) exhibited a morphologically normal glomerulus with normal basement membrane, capillaries and proximal convoluted tubule cellularity (Figure 3A). In contrast to the non-diabetic

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control rats, STZ-induced diabetic rat sections revealed a thickened basement membrane of both the glomerulus and the Bowman's capsule. In addition, the proximal convoluted tubule hypercellularity was observed following five weeks of study (Figure 3B). Treatment with transdermal insulin and sc insulin for five weeks resulted in attenuation of these anomalies when compared with untreated STZ-diabetic rats (Figure 3C and D). Figure 3(A) shows the normal glomerulus of the untreated non-diabetic rat kidney section showing normal glomerular basement membrane (GBM), capillaries (C), nuclei (N), proximal convoluted tubule (PCT), mesangium (M), veins (V) and squamous cells (S). Compared with

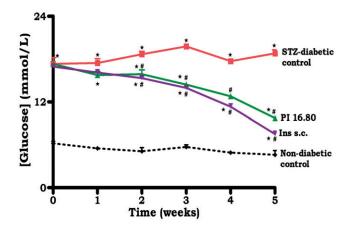


Figure 1. Comparison of mean weekly urinary glucose outputs of STZ-induced diabetic rats treated with sc insulin and PI hydrogel matrix patch (16.80 µg/kg) thrice daily at 09 h00 followed by the same dose at 17 h00 and the 8 h later (01h00) for five weeks with control non-diabetic rats and untreated STZ-induced diabetic rats. Notes: *Denotes p < 0.05 by comparison with non-diabetic control animals. #Denotes p < 0.05 by comparison with untreated STZ-induced diabetic animals.

the untreated non-diabetic control rats (Figure 3A), STZinduced diabetic rats (Figure 3B) showed thickened basement membrane of the Bowmans capsule (TBMBC), thickened glomerular basement membrane (TGBM) and hypercellularity of the proximal tubules (HCPT) after five weeks of the study. Treatment with insulin-containing dermal patches and sc insulin for five weeks however, attenuated these features when compared with the untreated STZ-diabetic rats (Figure 3C and D).

Discussion

The data presented herein show that transdermal application of PI matrix patches ameliorates kidney function of STZinduced diabetic rats. The findings are clinically relevant considering that the development and progression to ESRD, the principal cause of death as a result of diabetic nephropathy, is associated with a progressive decline in renal function. Several studies have reported compromised renal function in experimental diabetes^{10,11,21} and diabetic patients.^{14,22–25} The current therapeutic approach to diabetes using hypoglycemic agents has limited efficacy in averting the development of renal complications. Therefore, the findings are of considerable importance because they indicate that insulin-containing dermal patches may not only eliminate the frequent dosing administration associated with bolus injections, but also improve kidney function.

The effects of insulin over time are dependent on their pharmacokinetic and the mode of administration. Application of insulin-containing dermal patches delivers sustained controlled insulin to probably achieve physiological insulin concentration in the portal vein. The controlled sustained insulin release may reduce systemic hyperinsulinemia and, in

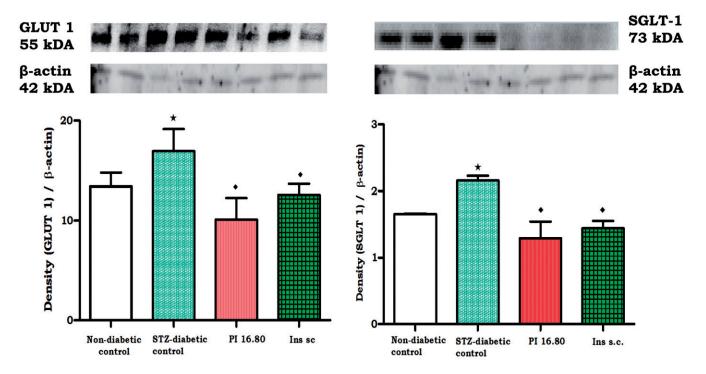


Figure 2. Comparison of the effects of topically applied PI hydrogel matrix patch and sc insulin on GLUT1 and SGLT1 in kidney tissues of STZ-induced diabetic rats, respectively, with untreated non-diabetic as determined by western blotting. Values are expressed as mean \pm SEM. Values were obtained from western blots for six preparations. Notes: *Denotes p < 0.05 by comparison with non-diabetic animals. *Denotes p < 0.05 by comparison with respective control animals.

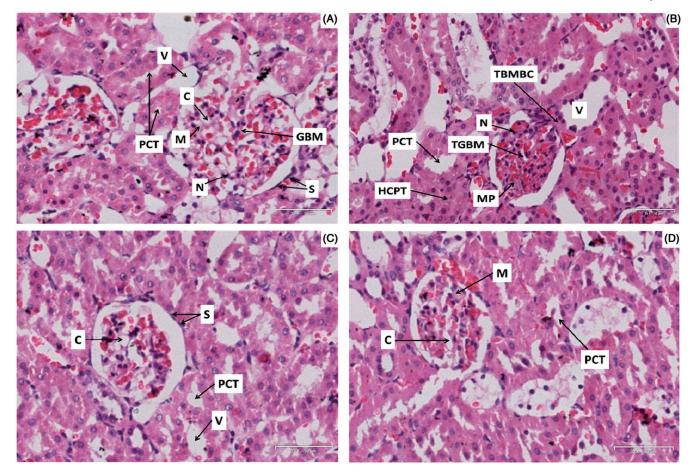


Figure 3. Photomicrographs (H and E) illustrating the effects of transdermally delivered insulin on the morphology of the kidney in STZ-induced diabetic rats. Photomicrograph (A) represents the normal glomerulus of the untreated non-diabetic rat kidney section showing normal glomerular basement membrane (GMB), glomerular capillaries (C), nuclei (N), proximal convoluted tubule (PCT), mesangium (M), veins (V) and squamous cells (S). Photomicrograph (B) represents the injured glomerulus of the STZ-diabetic rat showing irregular glomerular capillaries, thickened glomerular basement membrane (TGBM), thickened basement membrane of the Bowmans capsule (TBMBC), hypercellularity of the proximal tubules (HPT) and mesangial proliferation (MP). Photomicrograph (C) represents the glomerulus of the transdermal insulin treated rat kidney section showing irregular glomerular capillaries but no basement membrane thickening and mesangial proliferation. Photomicrograph (D) represents the glomerulus of the subcutaneous insulin treated rat kidney section showing irregular glomerular capillaries but no basement membrane thickening allowerular capillaries but no basement membrane thickening irregular glomerular capillaries but no basement membrane thickening (Mag $35 \times 100 \, \mu$ m).

the long run, insulin resistance by reversing down regulation of insulin receptors. On the other hand, bolus iv, sc or im insulin injections elicit relatively high plasma levels of insulin which are exposed to peripheral organs and probably cause hyperinsulinemic edema and hypertension.⁸ The invasive PI dermal patches may offer minimally invasive insulin delivery in clinical applications to perhaps improve insulin bioavailability and patient compliance.

STZ-induced diabetic rats exhibited marked weekly decreases in urinary Na⁺ excretion and elevated plasma creatinine concentration at the end of five weeks with concomitant reduction in GFR. We suggest that renal insufficiency in diabetic animals was not due to the STZ nephrotoxicity since the dose of STZ (60 mg/kg) used to induce diabetes has been reported to have minimal kidney toxicity in experimental animals.^{26–28} Na⁺ retention can also be attributed to diabetes-induced histopathological changes in the kidney particularly thickening of the glomerular basement membrane (Photomicrograph B) which decreases the filtration surface area. These changes are attributed in part to decreased insulin secretion (both type 1 and type 2 diabetes mellitus).²⁹

The kidney of STZ-induced diabetic rats showed structural changes (Photomicrograph C) which was prevented by dermal PI matrix patches treatment indicating protection of diabetes induced kidney damage. Treatment with insulin-containing dermal patches probably reduced renal damage to offset the renal effects associated hyperglycemia by mechanisms through a number of metabolic pathways. Insulin-containing dermal patches increased urinary Na⁺ excretion of STZinduced diabetic rats in contrast to hyperinsulinemic edema and hypertension due to increased Na⁺ retention associated with intensive insulin therapy.⁸ Our study shows that transdermal PI matrix patches can reverse the previously reported inability of the kidney to excrete Na^+ in STZ-diabetes mellitus.^{30–32} Hyperinsulinemic edema and hypertension associated with intensive insulin therapy have been attributed, at least in part, to Na⁺retaining action of insulin.⁸ However, literature evidence on the effects of insulin on kidney function in diabetes is conflicting and remains unclear. It would appear that renal effects of insulin depend on endogenous levels of circulating insulin and on the availability of insulin-binding sites in the kidney.³³ Indeed, physiological concentrations of insulin decrease renal Na⁺ re-absorption and prevent the rise

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in plasma K⁺ concentrations in diabetics^{34,35} while high doses increase plasma Na⁺ concentration and cause hypokalemia.³⁶ The results suggest that the pectin hydrogel dermal insulin matrix patches delivered physiologically relevant amounts of pharmacologically active insulin. Indeed, the glycemic control and amelioration of kidney function of STZ-induced rats observed in the present study were achieved with PI hydrogel matrix patches that elicited plasma insulin concentrations within the physiological range. The highest dose of PI hydrogel matrix patch (16.80 µg/kg) increased plasma insulin concentrations to levels comparable with non-diabetic animals and was effective in ameliorating renal fluid and electrolyte handling and expression of glucose transporters as well as reducing the mean arterial blood pressure of STZinduced diabetic rats. Studies indicate that hyperglycemia is the main cause of the decline in kidney function in diabetic patients.^{24,25} The changes attenuated by transdermal insulin treatment indicate beneficial effects on renal function in diabetes.

Glycosuria observed in untreated STZ-induced diabetic rats was ameliorated by transdermal insulin treatment as evidenced by the decrease of plasma glucose concentrations measured at the end of the experimental period. We have reported in another study that insulin-containing dermal patch formulation sustains slow controlled release of insulin into the bloodstream of diabetic rats with a concomitant reduction in plasma glucose concentrations.^{9,37} As assessed by western blotting, PI treatment significantly decreased the renal expression of SGLT1 and GLUT1 to perhaps to reduce glucose re-absorption. These transporters which were unregulated in untreated STZ-induced diabetic rats increased the reabsorption of glucose and thus contributed to the pre-existing hyperglycemia.^{16,17} Taken together, the studies suggest that insulin-containing dermal patches increase urinary Na⁺ excretion and decrease renal expression of glucose transporters of STZ-induced diabetic rats.

In summary, the current data suggest that topically administered insulin not only improves glycemic control and kidney function of STZ-induced diabetic rats, but also ameliorates the expression of renal insulin-stimulated facilitative glucose transporters. Therefore, this method of insulin delivery system may gradually progress towards physiological insulin replacement and reduce long-term complications of diabetes mellitus. The major limitations of the current study include lack of measurements of a wide range of humoral factors known to influence kidney function such as aldosterone, atrial natriuretic peptide and angiotensin II which would have enabled us to assess their involvement during the course of the treatment.

Declaration of interest

The authors declare that there is no interest that could be perceived as prejudicing the impartiality of the research reported.

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