



# Muscular forces affect the glycosaminoglycan content of joint cartilage

Unloading in human volunteers with the HEPHAISTOS lower leg orthosis

Bergita Ganse, Jochen Zange, Tobias Weber, Regina Pohle-Fröhlich, Bernd W Johannes, Matthias Hackenbroch, Jörn Rittweger, Peer Eysel & Timmo Koy

To cite this article: Bergita Ganse, Jochen Zange, Tobias Weber, Regina Pohle-Fröhlich, Bernd W Johannes, Matthias Hackenbroch, Jörn Rittweger, Peer Eysel & Timmo Koy (2015) Muscular forces affect the glycosaminoglycan content of joint cartilage, Acta Orthopaedica, 86:3, 388-392, DOI: [10.3109/17453674.2014.989382](https://doi.org/10.3109/17453674.2014.989382)

To link to this article: <https://doi.org/10.3109/17453674.2014.989382>



Copyright: © Nordic Orthopaedic Federation



Published online: 24 Nov 2014.



Submit your article to this journal [↗](#)



Article views: 832



View related articles [↗](#)



View Crossmark data [↗](#)



Citing articles: 2 View citing articles [↗](#)

# Muscular forces affect the glycosaminoglycan content of joint cartilage

## Unloading in human volunteers with the HEPHAISTOS lower leg orthosis

Bergita GANSE<sup>1,2</sup>, Jochen ZANGE<sup>1</sup>, Tobias WEBER<sup>1,3</sup>, Regina POHLE-FRÖHLICH<sup>4</sup>, Bernd W JOHANNES<sup>1</sup>, Matthias HACKENBROCH<sup>5</sup>, Jörn RITTWEGER<sup>1</sup>, Peer EYSEL<sup>6</sup>, Timmo KOY<sup>6</sup>

<sup>1</sup> Division Space Physiology, Institute of Aerospace Medicine, German Aerospace Center (DLR), Cologne; <sup>2</sup> Department of Orthopaedic Trauma, RWTH Aachen University, Aachen; <sup>3</sup> Space Medicine Office, Directorate of Human Spaceflight and Operations (D/HSO), European Astronaut Center, European Space Agency, Cologne; <sup>4</sup> Institute for Pattern Recognition, Hochschule Niederrhein, Krefeld; <sup>5</sup> Department of Radiology and <sup>6</sup> Department of Orthopaedic and Trauma Surgery, University of Cologne, Cologne, Germany.

Correspondence: bergita.ganse@dlr.de

Submitted 2014-07-02. Accepted 2014-09-27.

**Background and purpose** — Unloading alters the thickness of joint cartilage. It is unknown, however, to what extent unloading leads to a loss of glycosaminoglycans (GAGs) in the cartilage tissue. We hypothesized that muscle forces, in addition to axial loading, are necessary to maintain the joint cartilage GAG content of the knee and the upper and lower ankle.

**Patients and methods** — The HEPHAISTOS orthosis was worn unilaterally by 11 men (mean age 31 (23–50) years old) for 56 days. The orthosis reduces activation and force production of the calf muscles while it permits full gravitational loading of the lower leg. MRI measurements of the knee and ankle were taken before the intervention, during the intervention (on day 49), and 14 days after the end of the intervention. Cartilage segmentation was conducted semiautomatically for the knee joint (4 segments) and for the upper (tibio-talar) and lower (subtalar) ankle joints (2 segments each). Linear mixed-effects (LME) models were used for statistical analysis.

**Results** — 8 volunteers completed the MRI experiment. In the lower ankle joint, differences in  $\Delta T_1$  were found between the end of the intervention and 14 days after ( $p = 0.004$ ), indicating a decrease in GAG content after reloading. There were no statistically significant differences in  $\Delta T_1$  values in the knee and upper ankle joints.

**Interpretation** — Our findings suggest that in addition to gravitational load, muscular forces affect cartilage composition depending on the local distribution of forces in the joints affected by muscle contraction.

Unloading has been shown to cause a decrease in cartilage thickness (Vanwanseele et al. 2002a, b, Hinterwimmer et al. 2004, Eckstein et al. 2006, Liphardt et al. 2009, Wang et al. 2010) and is thought to lead to a loss of glycosaminoglycans (GAGs) in cartilage tissue (Bashir et al. 1996, 1999). Reduced GAG content may be interpreted as an early sign of cartilage degeneration (Bashir et al. 1996). Cartilage is known to be sensitive to mechanical strain, but it is unclear how far axial loading, shear forces, and the pull of the muscles on bone contribute to the adaptation of joint cartilage GAG content to unloading.

To investigate the effects of selective muscular unloading during normal gravitational load on the lower limb, the HEPHAISTOS orthosis was developed and tested in an ambulatory clinical interventional study (the HEP study). During walking and standing, the orthosis substantially reduces the activation of the calf muscles and the production of force on the forefoot in the plantar direction, while it permits full gravitational loading of the ankle joint and the lower leg (Weber et al. 2013a). It has been shown that muscle contractions have a key role in generation of strain in bone during locomotion, and are therefore crucial for mechano-adaptation of bone (Rittweger 2008).

Increased joint cartilage thickness, as found in athletes (Eckstein 2014), improves cushioning and protects against wear-off. Cartilage thickness is known to depend on both mechanical and biochemical factors (Niehoff et al. 2011).

We investigated the effects of chronically reduced forces produced by the plantar flexors, in combination with normal axial weight loading, on joint cartilage. The unique feature of

the study was that the orthosis enabled us to reduce muscular forces while keeping gait and load normal. Delayed gadolinium-enhanced MRI of cartilage (dGEMRIC) was chosen to assess changes in the cartilage tissue (Bashir et al. 1996, 1997, 1999, Burstein et al. 2001). We used a standard MRI hardware protocol for dGEMRIC imaging. This protocol has been applied to knee joint cartilage in a large number of studies (Bashir et al. 1996, 1997, 1999, Burstein et al. 2001, Mayerhoefer et al. 2010) and to the upper ankle joint in only a few studies so far (Domayer et al. 2010, Wiewiorski et al. 2013). dGEMRIC measurements of the lower ankle joint have not been published before, probably because they are technically more demanding.

We hypothesized that a chronic reduction of plantar flexion forces would result in a reduction in GAG content in the cartilage of the ankle joints and the knee. We also hypothesized that joints that are normally loaded to a higher degree by calf muscle contraction would react on calf muscle unloading to a greater extent than those joints that are less influenced by calf muscle contractions. Thus, effects would be expected to be greatest in the lower ankle joint followed by the upper ankle joint. Only small effects, if any, would be expected in the knee joint.

## Material and methods

### Study setting

The HEPHAISTOS study (HEP study) was conducted at the German Aerospace Center in Cologne, Germany, and is registered at [www.clinicaltrials.gov](http://www.clinicaltrials.gov) (identifier: NCT01576081). It was approved by the Ethics Committee of the Northern Rhine Medical Association (Ärzttekammer Nordrhein, Düsseldorf, Germany, no. 2010169). Out of 11 men (mean age 31 (23–50) years) who wore the orthosis unilaterally for 56 days, 8 completed the MRI experiment presented here. 2 volunteers had to be excluded from further MRI measurements after showing symptoms of contrast-agent intolerance and 1 refused to participate in the MRI measurements. The study protocol and details of the organization, schedule, and methods of the HEP study have already been published by Weber et al. (2013a).

### The HEPHAISTOS orthosis

The orthosis causes unloading of the calf muscles while permitting a near to normal gait, thus maintaining full impact of the body mass on the ankle and the lower leg (Figure 1). It substantially reduces plantar flexor torque and muscle activation (measured by electromyography), and it affects arterial diameter (measured by ultrasound) (Weber et al. 2013a, b, 2014). When the orthosis is worn, normal movement in the knee joint is possible. Flexion and extension are limited in the upper ankle joint, while supination and pronation of the lower ankle joint are not possible. Tibio-talar forces are reduced by three-quarters, while femoro-tibial forces are unaltered when wearing HEPHAISTOS. Force development of the gastrocne-

mus muscle and its pull on the calcaneus through the Achilles tendon are reduced by the absence of counter-forces on the forefoot (unpublished observations). The mechanical role of the ankle during walking is taken over by a metallic joint below the foot with an integrated spring that replaces the role of the calf muscle. To investigate the influence of the orthosis on joint cartilage, we analyzed the knee joint and the upper (tibio-talar) and lower (subtalar) ankle joints. The orthosis was manufactured individually for each subject by ORTEMA GmbH (Markgröningen, Germany). The volunteers had to wear the HEPHAISTOS orthosis for 56 days, during all locomotive activities that required loading of the leg. The following link leads to the webpage of the DLR with a video clip presenting the HEPHAISTOS unloading orthosis: [http://www.dlr.de/me/en/desktopdefault.aspx/tabid-7389/12432\\_read-35410/](http://www.dlr.de/me/en/desktopdefault.aspx/tabid-7389/12432_read-35410/).

### The dGEMRIC protocol

MRI scans were done according to the dGEMRIC protocol (Mayerhoefer et al. 2010). Each volunteer underwent MRI scans of the ankle and knee of the intervention leg before the intervention (BDC), on day 49 of the intervention (HEP49), and 14 days after the end of the intervention phase (R+14). Each time, MRI scans were performed before and after intravenous administration of the gadolinium-based contrast agent Gd-DOTA (Dotarem; gadoteric acid, 0.4 mg per kg body mass).

### MRI

MRI scans of the ankle and the knee were obtained with a knee coil in a 3T MRI scanner (Achieva; Philips Medical Systems). Measurements were taken with 2 flip angles of 5° and 25°, and calculations were performed according to Mayerhoefer et al. (2010). Signal intensities were calculated for each pixel and intensities were corrected from a B1-map (map of relative pulse angles). Scaling of maps was adjusted and T1 was calculated pixel-wise. Each ankle measurement was planned with a series of cross-sectional images based on sagittal pilot images. From the ankle, 2 individual slices were analyzed with a 160 × 160 mm field of view, an acquisition matrix of 704 × 704 pixels, and 3 mm slice thickness. From the knee, 2 individual slices were analyzed with a 160 × 160 mm field of view, an acquisition matrix of 560 × 560 pixels, and 3 mm slice thickness.

### Calculation of $\Delta T_1$ values and segmentation

Segmentation was performed semiautomatically for the areas shown in Figure 2. This means that a ROI was first set manually, and a threshold algorithm was applied to the selected region before the cartilage region was defined by region-growing. The knee joint cartilage was subdivided into 4 segments of equal height for analysis. For the ankle joints, a proximal segment and a distal segment of equal height were selected. The ankle joint cartilage was not thick enough for the analysis of more subsegments in the resolution available.



Figure 1. The HEPHAISTOS orthosis.

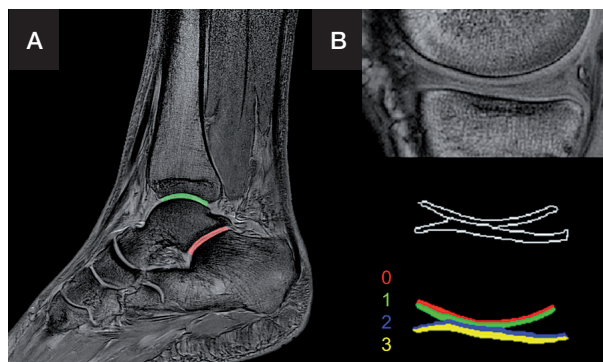


Figure 2. Segmentation of the upper (green) and lower (red) ankle joint (articulatio subtalaris) with a distal and a proximal segment each (panel A), and the knee joint (segments 0–3) (panel B).

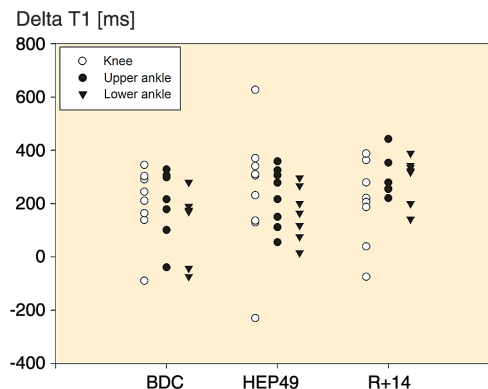


Figure 3.  $\Delta T_1$  values in the course of the study, in each joint for each volunteer. The baseline measurement was taken before the intervention (baseline data collection, BDC), the second measurement was on day 49 of the intervention (HEPHAISTOS, HEP49), and the third measurement was 14 days after the end of the intervention (recovery, R+14).  $\Delta T_1$  indicates the GAG content (lower  $\Delta T_1$  values reflect higher GAG content).

## Statistics

IBM SPSS Statistics release 20.0.0 was used to calculate linear mixed-effects (LME) models with segment, measurement, and their interaction as fixed effects and subjects as a random effect (variance components). Significance was assumed at  $p < 0.05$ . The assumptions made were a normal distribution of the raw data and the residuals. The Kolmogorov-Smirnov test showed a normal distribution of  $\Delta T_1$  values in the cartilage of the upper ankle joint ( $p = 0.6$ , residuals  $p = 0.9$ ), the lower ankle joint ( $p = 0.8$ , residuals  $p = 0.6$ ), and the knee ( $p = 0.9$ , residuals  $p = 0.4$ ). Data are presented as counts with their SD. Exclusion conditions were  $\Delta T_1$  times of  $< 400$  ms and  $> 1,500$  ms. SigmaPlot software version 12.0 was used to plot data.  $\Delta T_1$  was the primary outcome measure of this study. An increase in  $\Delta T_1$  corresponded to a decrease in the GAG content.

## Results

An overview of average  $\Delta T_1$  values for each site and each measurement is provided in Figure 3. Further details are shown in Figure 4.

### The knee joint

The LME model revealed a significant difference in  $\Delta T_1$  values between segments ( $p < 0.001$ ) but no statistically significant difference between measurements, either for the entire knee cartilage ( $p = 0.5$ ) or for the interaction with the individual segments ( $p = 0.9$ ). Throughout the study, cartilage closer to the bone had lower  $\Delta T_1$  values than cartilage further away from the bone.

### The upper ankle joint

There was no statistically significant difference between the  $\Delta T_1$  values of the 2 segments (proximal and distal,  $p = 0.4$ ).

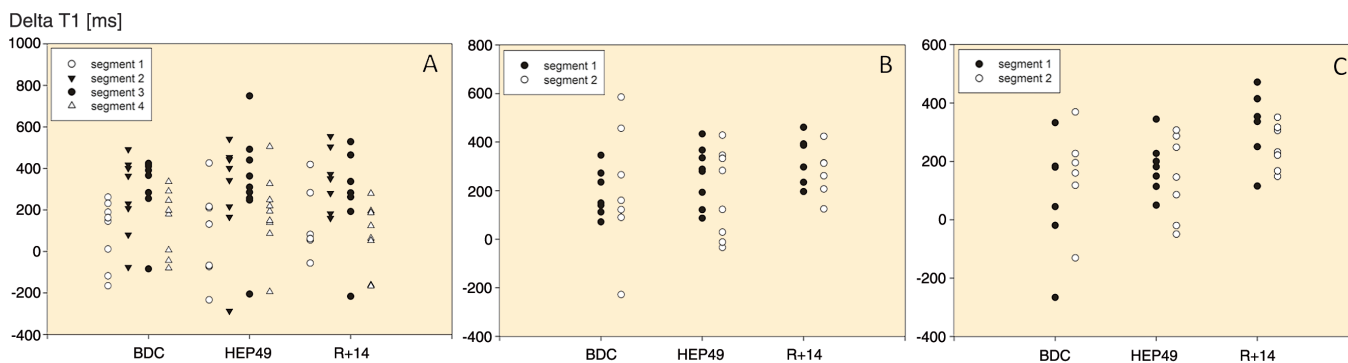


Figure 4.  $\Delta T_1$  values of the separate segments of the knee joint (A), the upper ankle joint (B) and the lower ankle joint (C) in the individual volunteers throughout the course of the study. In the knee joint, values differ significantly among segments ( $p < 0.001$ ).  $\Delta T_1$  indicates the GAG content (lower  $\Delta T_1$  values reflect higher GAG content).



or between measurements ( $p = 0.2$ ). The interaction between segment and measurement was not significant either ( $p = 0.7$ ).

### **The lower ankle joint**

We found a difference in  $\Delta T_1$  values between measurements, with higher  $\Delta T_1$  after the intervention than before ( $p = 0.004$ ). The effect occurred after reloading.  $\Delta T_1$  values were similar when comparing the proximal and distal segment ( $p = 0.7$ ), and no statistically significant differences could be found when we analyzed the interaction between segment and measurement ( $p = 0.2$ ).

## **Discussion**

The HEPHAISTOS orthosis makes it possible to investigate the effects of widely inactive lower leg muscles during normal gravitational load patterns as experienced in everyday life, without any substantial change in gravitational and mass-inertial skeletal forces (Weber et al. 2013a). Our main findings were as follows. (1) A decrease in GAG content of the lower ankle (subtalar) joint cartilage was found to occur not during the intervention, but after reloading. (2) Axial load alone was sufficient to maintain the cartilage GAG content of the upper ankle joint. The GAG content of the knee joint cartilage was not affected either. (3) The dGEMRIC method can be applied to the lower ankle joint.

### **Observations in the literature**

The dGEMRIC protocol was initially developed to assess the glycosaminoglycan content of knee joint cartilage (Bashir et al. 1996, 1997, 1999, Burstein et al. 2001). The dGEMRIC method was recently applied to the upper ankle joint (Domayer et al. 2010, Wiewiorski et al. 2013). To our knowledge, the dGEMRIC method has not been applied to the lower ankle joint before, probably because the cartilage is thin and segmentation is technically difficult. We found that the dGEMRIC protocol can be used to assess relative changes in the GAG content of the lower ankle joint, which may be of interest for research in foot and ankle surgery as well as for rheumatology.

Unloading has been shown to reduce cartilage thickness (Eckstein et al. 2014). By analyzing MRI images taken before and after 14 days of 6° head down tilt bed rest in human subjects, Liphardt et al. (2009) showed that the articular knee cartilage thickness is sensitive to unloading. They found a substantial decrease in thickness of the tibial knee joint cartilage but not in the thickness of femoral knee joint cartilage. Wang et al. (2010) performed a 4-week tail suspension study on rats and found decreases in cartilage thickness of the patella and the medial femoral condyle. Vanwanseele et al. (2002a, b) found progressive thinning of the knee cartilage in patients with spinal cord injuries. Hinterwimmer et al. (2004) showed thinning of articular cartilage already after 7 weeks of par-

tial load bearing. Regarding cartilage thickness, changes were usually found to occur throughout unloading and not after reloading.

Mayerhoefer et al. (2010) analyzed the effect of 15 min of unloading of the knee joint on T1-Gd with the dGEMRIC method and found that there was no statistically significant effect on T1-Gd relaxation times. Long-term unloading of human joint cartilage has not, however, been investigated previously with this method. The effects of selective muscular unloading on joint cartilage during normal weight bearing had also not been investigated before our study. One might think that the GAG content decreases during unloading, just as cartilage thickness has been shown to decrease. Our results, however, indicate that a decrease in glycosaminoglycan content may occur after reloading following muscular inactivation, depending on the joint location and the type of immobilization. It remains unclear, however, whether reloading causes remodeling or whether remodeling is just delayed and takes a while to occur. Other studies have shown changes in GAG content in cartilage tissue to occur within a few weeks (Roos et al. 2005, Van Ginckel et al. 2010). However, the timing of changes in joint cartilage GAG content remains unclear. Increased  $\Delta T_1$  is thought to be correlated with reduced glycosaminoglycan content, and it is usually interpreted as a sign of early degeneration (Bashir et al. 1996, 1999). Our findings indicate that degeneration of joint cartilage might in some cases follow reloading after a longer period of unloading. Future studies in this field should therefore include a follow-up period after reambulation.

### **Possible reasons for asymmetrical findings**

HEPHAISTOS unloads the ankle, but not the knee. When the orthosis is worn, normal movement is possible in the knee joint while flexion and extension are limited in the upper ankle joint and supination and pronation are not possible in the lower ankle joint. The subtalar joint has an angle of 30–40° to the horizontal line. Supination and pronation are the possible movements of the subtalar joint, and both are made impossible while wearing HEPHAISTOS. The subtalar joint is therefore almost completely immobilized by the orthosis, while the upper ankle joint is only partially restricted (extension and flexion of the ankle) and the knee joint is not restricted at all. Furthermore, tibial forces are known to load eccentrically on the calcaneus, leading to torque and shear stresses in the joint. Forces are not distributed homogeneously throughout the articular surface of the subtalar joint (Mueller et al. 2014). In cases in which the stabilizing muscles were atrophied after the intervention, shear stresses may have exceeded their normal extent and led to cartilage impairment.

### **Clinical relevance of our findings**

Considering our results, a reduction in the GAG content of cartilage following reloading after cast immobilization and after nonoperative treatment of conditions such as Achilles

tendon ruptures appears to be possible and should be investigated further. The same effects may also follow immobilization in an external fixator. The findings may fuel the ongoing discussions for or against nonoperative and operative treatment options in a number of conditions (Cohen and Balcom 2003, Jiang et al. 2012). For these considerations, it would be of interest to know how long the reduction in GAGs lasts, how its timely development takes place, and the degree to which it is reversible. Furthermore, it is important to identify joints that are particularly vulnerable and unloading patterns that prevent changes in cartilage.

BG: analysis and interpretation of the data, drafting of the article, and assembly of data. JZ: conception and design, and analysis and interpretation of the data. TW: organization of study and recruitment of subjects. RPF: segmentation and data processing. BWJ: statistical analysis. MH: technical support (MRI) and radiology expertise. JR: obtaining of funding, and conception and design. PE: administrative support. TK: conception and design, and collection of data.

We thank the volunteers for participating willingly in the study. Special thanks to Jonas Reck who helped to organize the experiments.

No competing interests declared.

- Bashir A, Gray M L, Burstein D. Gd-DTPA2- as a measure of cartilage degradation. *Magn Reson Med* 1996; 36 (5): 665-73.
- Bashir A, Gray M L, Boutin R D, Burstein D. Glycosaminoglycan in articular cartilage: in vivo assessment with delayed Gd(DTPA)(2-)-enhanced MR imaging. *Radiology* 1997; 205 (2): 551-8.
- Bashir A, Gray M L, Hartke J, Burstein D. Nondestructive imaging of human cartilage glycosaminoglycan concentration by MRI. *Magn Reson Med* 1999; 41 (5): 857-65.
- Burstein D, Velyvis J, Scott K T, Stock K W, Kim Y J, Jaramillo D et al. Protocol issues for delayed Gd(DTPA)(2-)-enhanced MRI (dGEMRIC) for clinical evaluation of articular cartilage. *Magn Reson Med* 2001; 45: 36-41.
- Cohen R S, Balcom T A. Current treatment options for ankle injuries: lateral ankle sprain, Achilles tendonitis, and Achilles rupture. *Curr Sports Med Rep* 2003; 2 (5): 251-4.
- Domayer S E, Trattinig S, Stelzeneder D, Hirschfeld C, Quirbach S, Dorotka R et al. Delayed gadolinium-enhanced MRI of cartilage in the ankle at 3 T: feasibility and preliminary results after matrix-associated autologous chondrocyte implantation. *J Magn Reson Imaging* 2010; 31 (3): 732-9.
- Eckstein F, Hudelmaier M, Putz R. The effects of exercise on human articular cartilage. *J Anat* 2006; 208: 491-512.
- Eckstein F, Boeth H, Diederichs G, Wirth W, Hudelmaier M, Cotofana S et al. Longitudinal change in femorotibial cartilage thickness and subchondral bone plate area in male and female adolescent vs. mature athletes. *Ann Anat* 2014; 196 (2-3): 150-7.

- Hinterwimmer S, Krammer M, Kroetz M, Glaser C, Baumgart R, Reiser M et al. Cartilage atrophy in the knees of patients after seven weeks of partial load bearing. *Arthritis Rheum* 2004; 50 (8): 2516-20.
- Jiang N, Wang B, Chen A, Dong F, Yu B. Operative versus nonoperative treatment for acute Achilles tendon rupture: a meta-analysis based on current evidence. *Int Orthop* 2012; 36 (4): 765-73.
- Liphardt A M, Mündermann A, Koo S, Baecker N, Andriacchi T P, Zange J et al. Vibration training intervention to maintain cartilage thickness and serum concentrations of cartilage oligomeric matrix protein (COMP) during immobilization. *Osteoarthritis Cartilage* 2009; 17 (12): 1598-603.
- Mayerhoefer M E, Welsch H G, Mamisch T C, Kainberger F, Weber M, Nemec S et al. The in vivo effects of unloading and compression on T1-Gd (dGEMRIC) relaxation times in healthy articular knee cartilage at 3.0 Tesla. *Eur Radiol* 2010; 20: 443-449.
- Mueller F, Hoechel S, Klawns J, Wirz D, Mueller-Gerbl M. The subtalar and talonavicular joints: a way to access the long-term load intake using conventional CT-data. *Surg Radiol Anat* 2014; 36 (5): 463-72.
- Niehoff A, Müller M, Brüggemann L, Savage T, Zaucke F, Eckstein F et al. Deformational behaviour of knee cartilage and changes in serum cartilage oligomeric matrix protein (COMP) after running and drop landing. *Osteoarthritis Cartilage* 2011; 19 (8): 1003-10.
- Rittweger J. Ten years muscle-bone hypothesis: what have we learned so far? - almost a festschrift-. *J Musculoskelet Neuronal Interact* 2008; 8 (2): 174-8.
- Roos E M, Dahlberg L. Positive effects of moderate exercise on glycosaminoglycan content in knee cartilage: a four-month, randomized, controlled trial in patients at risk of osteoarthritis. *Arthritis Rheum* 2005; 52(11): 3507-14.
- Vanwanseele B, Eckstein F, Knecht H, Stussi E, Spaepen A. Knee cartilage of spinal cord-injured patients displays progressive thinning in the absence of normal joint loading and movement. *Arthritis Rheum* 2002a; 46: 2073-8.
- Vanwanseele B, Lucchinietti E, Strussi E. The effects of immobilization on the characteristics of articular cartilage: current concepts and future directions. *Osteoarthritis Cartilage* 2002b; 10: 408-19.
- Van Ginckel A, Baelde N, Almqvist K F, Roosen P, McNair P, Witvrouw E. Functional adaptation of knee cartilage in asymptomatic female novice runners compared to sedentary controls. A longitudinal analysis using delayed Gadolinium Enhanced Magnetic Resonance Imaging of Cartilage (dGEMRIC). *Osteoarthritis Cartilage* 2010; 18(12): 1564-9.
- Wang Q, Zheng Y P, Wang X Y, Huang Y P, Liu M Q, Wang S Z et al. Ultrasound evaluation of site-specific effect of simulated microgravity on articular cartilage. *Ultrasound Med Biol* 2010; 36 (7): 1089-97.
- Weber T, Ducos M, Mulder E, Herrera F, Brüggemann GP, Bloch W et al. The specific role of gravitational accelerations for arterial adaptations. *J Appl Physiol* 2013a; 114 (3): 387-93.
- Weber T, Ducos M, Yang P-F, Jos D, Frings-Meuthen P, Brüggemann G-P et al. The HEPHAISTOS study: Compliance, adherence and rehabilitation with a novel orthotic device for calf muscle silencing. *J Musculoskelet Neuron Interact* 2013b; 13 (4): 487-495.
- Weber T, Ducos M, Mulder E, Beijer A, Herrera F, Zange J et al. The relationship between exercise-induced muscle fatigue, arterial blood flow and muscle perfusion after 56 days local muscle unloading. *Clin Physiol Funct Imaging* 2014; 34 (3): 218-29.
- Wiewiorski M, Miska M, Kretzschmar M, Studler U, Bieri O, Valderrabano V. Delayed gadolinium-enhanced MRI of cartilage of the ankle joint: results after autologous matrix-induced chondrogenesis (AMIC)-aided reconstruction of osteochondral lesions of the talus. *Clin Radiol* 2013; 68 (10): 1031-8.